

Faculty of Electrical Engineering

SPECTRAL ESTIMATION AND SUPERVISED CLASSIFICATION TECHNIQUE FOR REAL TIME ELECTROMYOGRAPHY PATTERN RECOGNITION

Nuradebah binti Burhan

Master of Science in Electrical Engineering

SPECTRAL ESTIMATION AND SUPERVISED CLASSIFICATION TECHNIQUE FOR REAL TIME ELECTROMYOGRAPHY PATTERN RECOGNITION

NURADEBAH BINTI BURHAN

A thesis submitted in fulfillment of the requirements for the award of the degree of Master of Science in Electrical Engineering

Faculty of Electrical Engineering

UNIVERSITI TEKNIKAL MALAYSIA MELAKA

2018

DECLARATION

I declare that this thesis entitled "Spectral Estimation and Supervised Classification
Technique for Real Time Electromyography Pattern Recognition" is the result of my own
research except as cited in the references. The thesis has not been accepted for any degree
and is not concurrently submitted in candidature of any other degree.

Signature	:	
Name	:	
Date	:	

APPROVAL

I hereby declare that I have read	i this the	esis and in my opinion this thesis is sufficient in term			
of scope and quality for the award of Master of Science in Electrical Engineering.					
Signature	:				
Supervisor Name	:				
Date	:				

DEDICATION

To my beloved mother and father

ABSTRACT

Electromyography (EMG) signal is a biomedical signal which measures physical activity of human muscle. It has been acknowledged to be widely used in rehabilitation or recovery application system assisting physiotherapist to monitor a patient's physical strength, function, motion and overall well-being by addressing the underlying physical issues. In application system associated with rehabilitation, a signal processing and classification techniques are implemented to classify EMG signal obtained. For real time application in the rehabilitation, the classification is crucial issue. The success of the signal classification depends on the selection of the features that represent a raw EMG signal in the signal processing. Therefore, a robust and resilient denoising method and spectral estimation technique have been acknowledged as necessary to distinguish and detect the EMG pattern. The present study was undertaken to determine the characteristic of EMG features using denoising method and spectral estimation technique for assessing the EMG pattern based on a supervised classification algorithm. In the study, the combination of time-frequency domain (TFD) and time domain (TD) were identified as the preferred denoising method and spectral estimation techniques. In the first part of study, the recorded EMG signal filtered the contaminated noise by using wavelet transform (WT) approach which implemented discrete wavelet transform (DWT) method of the wavelet-denoising signal. Subsequently, the filtered signal containing useful information was extracted by three methods – root mean square (RMS), mean absolute value (MAV), and autoregressive (AR) covariance, all of which are commonly used in TD. A comparative analysis of the three different techniques was performed based on the accuracy performance of the EMG pattern classification using linear vector quantization (LVQ) neural network. In the experimental work undertaken, six healthy subjects comprised of males and females were selected. Three sets of resistance band loads, namely 5 kg, 9 kg, and 16 kg, were used as a force during the biceps brachii muscle contraction in the rehabilitation exercise. Each of the subject was required to perform three levels of the arm angle positions (30°, 90°, and 150°) for each set of resistance band load. The results of the experiment showed that Daubechies (db6) was the most appropriate DWT method including a 6-level decomposition, upholding soft rigrsure and heursure threshold rules, and a single-level threshold rescaling for the wavelet denoising signal analysis. From the three different techniques in extract feature vector as an input for LVQ classifier, the study concluded that the best system performance was the AR covariance method, where it obtained the average percentage of 95.56% for all classes in the EMG pattern recognition.

ABSTRAK

Isyarat elektromiografi (EMG) adalah satu isyarat biomedikal yang mengukur aktiviti fisikal otot manusia. Ia telah diterima umum sebagai satu aplikasi yang digunakan secara meluas dalam sistem rehabilitasi atau pemulihan bagi membantu ahli fisioterapi memantau kekuatan fisikal, fungsi, pergerakan dan kesejahteraan umum dengan menangani isu semasa fizikal pesakit berkenaan. Dalam sistem aplikasi berkaitan dengan pemulihan, teknik pemprosesan isyarat dan pengkelasan dilaksanakan untuk mengkategorikan isyarat EMG yang diperolehi. Untuk aplikasi masa nyata dalam pemulihan, klafikasi adalah isu penting. Kejayaan pengiktirafan isyarat bergantung pada pemilihan ciri-ciri yang mewakili isyarat EMG asli dalam pemprosesan isyarat. Oleh itu, satu kaedah pengkhususan yang teguh dan bingkas adalah dianggap perlu untuk meminimumkan bunyi. Kajian ini dijalankan untuk mengenal pasti ciri-ciri EMG dengan menggunakan kaedah pembuangan gangguan bunyi dan teknik anggaran spektrum untuk menilai corak EMG berdasarkan algoritma klasifikasi yang dipantau. Teknik optimum yang diperolehi telah dilaksanakan dalam sistem pemulihan masa yang nyata. Dalam kajian ini, gabungan domain masa-frekuensi (TFD) dan domain masa (TD) adalah kaedah pilihan untuk pembuangan gangguan bunyi dan teknik anggaran spektrum. Di bahagian pertama kajian, isyarat EMG yang dirakam telah ditapis daripada bunyi yang tercemar dengan menggunakan pendekatan transformasi gelombang kecil (WT) yang melaksanakan kaedah transformasi gelombang kecil diskret (DWT) dalam isyarat pembuangan gangguan bunyi-wavelet. Selepas daripada itu, isyarat yang ditapis yang mengandungi maklumat yang berguna telah diekstrak dengan menggunakan tiga kaedah yang biasa digunakan dalam TD iaitu punca min kuasa dua (RMS), nilai mutlak min (MAV), dan kovarians autoregresif (AR). Analisis perbandingan keatas tiga teknik berbeza telah dilakukan berdasarkan prestasi ketepatan klasifikasi pola EMG dengan menggunakan rangkaian neutral linear vector quantization (LVQ). Dalam melaksanakan kajian ini, enam subjek yang sihat terdiri daripada lelaki dan perempuan telah dipilih. Tiga set beban band rintangan, iaitu 5 kg, 9 kg, dan 16 kg, yang digunakan sebagai daya semasa pengecutan otot biseps brakii dalam latihan pemulihan berkenaan. Setiap subjek diperlukan untuk melaksanakan tiga peringkat posisi sudut lengan (30°, 90°, dan 150°) bagi setiap set beban band rintangan. Keputusan eksperimen menunjukkan bahawa Daubechies6 (db6) adalah kaedah DWT yang paling sesuai bersama dengan tahap penguraian 6 dengan pengekalan tahap rigrsure lembut dan peraturan ambang batas, dan tahap tunggal ambang untuk analisis pembuangan gangguan bunyi isyarat gelombang kecil. Daripada tiga teknik yang berbeza dalam vektor ciri ekstrak sebagai input untuk pengkelasan LVQ, kajian mendapati hasil sistem yang terbaik adalah kaedah kovarians AR, di mana ia memperolehi peratusan purata 95.56% untuk semua kelas dalam pengenalpastian pola EMG.

ACKNOWLEDGEMENTS

First and foremost, I would like to take this opportunity to express my sincere acknowledgement to my supervisor Dr. Rozaimi bin Ghazali from Faculty of Electrical Engineering at Universiti Teknikal Malaysia Melaka (UTeM) for his essential supervision, support, and encouragement towards the completion of this thesis.

I would like also to express my greatest to Ir. Mohammad 'Afif bin Kasno from Faculty of Engineering Technology, co-supervisor of this project for his advice and suggestion of this project.

Special thanks to Ministry of Higher Education (MOHE) and Universiti Teknikal Malaysia Melaka (UTeM) grant funding for the financial support throughout this project. This research is funded by the Research Acculturation Grant Scheme (RAGS) Grant No. RAGS/1/2015/TK05/FTK/03/B00112. Besides, I also would like to express my deepest gratitude to all peers and my parents for their moral support in completing this master. Lastly, thank you to everyone who had been to the crucial parts of realization of this project. Not forgetting, my humble apology as it is beyond my reach personally mentioned those who are involved directly or indirectly one to one.

TABLE OF CONTENTS

DECLARATION APPROVAL DEDICATION ABSTRACT ABSTRAK ACKNOWLEDGEMENTS TABLE OF CONTENTS LIST OF TABLES LIST OF TABLES LIST OF FIGURES LIST OF APPENDICES LIST OF SYMBOLS LIST OF SYMBOLS LIST OF PUBLICATIONS XXII LIST OF PUBLICATIONS XXII CHAPTER 1. INTRODUCTION 1.1 Project Background 1.2 Problem statement 1.3 Research Objectives 1.4 Scope of Research 1.5 Contribution of Research 1.6 Thesis Organization 2. LITERATURE REVIEW 2.1 Electromyography Measurement 2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2 Sources of Noise in Electromyography Technique 2.1.3 I Time Domain Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Transform 2.4 EMG Pattern Classification 2.5 EMG Rehabilitation Application on Biceps Brachii Muscle 2.6 Summary 48 3. METHODOLOGY 3.1 Experimental Design 3.3 Subjects and EMG Recording Procedure				PAGE
DEDICATION ABSTRACT	DE	CLAI	RATION	
ABSTRACT ABSTRAK ACKNOWLEDGEMENTS TABLE OF CONTENTS III TABLE OF CONTENTS IV LIST OF TABLES LIST OF TABLES LIST OF APPENDICES LIST OF ABBREVIATIONS LIST OF SYMBOLS LIST OF PUBLICATIONS CHAPTER 1. INTRODUCTION 1.1 Project Background 1.2 Problem statement 1.3 Research Objectives 1.4 Scope of Research 1.5 Contribution of Research 1.6 Thesis Organization 2. LITERATURE REVIEW 2.1 Electromyography Measurement 2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2. Sources of Noise in Electromyography Technique 2.3.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3.1 Time-Frequency Domain Feature Extraction 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.4 Experimental Design 3.5 METHODOLOGY 3.1 Experimental Design				
ABSTRAK ACKNOWLEDGEMENTS TABLE OF CONTENTS LIST OF TABLES VILIST OF TABLES VILIST OF APPENDICES LIST OF APPENDICES LIST OF APPENDICES LIST OF APPENDICES VILIST OF PUBLICATIONS VILIST OF PUBLICATIONS VILIST OF PUBLICATIONS CHAPTER 1. INTRODUCTION 1.1 Project Background 1.2 Problem statement 1.3 Research Objectives 1.4 Scope of Research 1.5 Contribution of Research 1.6 Thesis Organization 2. LITERATURE REVIEW 2.1 Electromyography Measurement 2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3.1 Time Domain Feature Extraction 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Transform 3.4 Experimental Design 3. METHODOLOGY 3.1 Experimental Design				
ACKNOWLEDGEMENTS TABLE OF CONTENTS LIST OF TABLES LIST OF FIGURES LIST OF APPENDICES LIST OF APPENDICES LIST OF ABBREVIATIONS LIST OF SYMBOLS LIST OF PUBLICATIONS LIST OF PUBLICATIONS CHAPTER 1. INTRODUCTION 1.1 Project Background 1.2 Problem statement 1.3 Research Objectives 1.4 Scope of Research 1.5 Contribution of Research 1.6 Thesis Organization 1.0 Thesis Organization 1.1 Invasive Electromyography Technique 2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.4 Experimental Design 3.5 METHODOLOGY 3.1 Experimental Design 4.9				
TABLE OF CONTENTS iv LIST OF TABLES vi LIST OF FIGURES ix LIST OF APPENDICES xii LIST OF ABBREVIATIONS xiii LIST OF SYMBOLS xvi LIST OF PUBLICATIONS xvi CHAPTER 1 1. INTRODUCTION 1 1.1. Project Background 1 1.2 Problem statement 8 1.3 Research Objectives 9 1.4 Scope of Research 9 1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 12 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3 I Time Domain Feature Extraction 22 2.3.1 Time Domain Feature Extraction 25 2.3.2 Frequency Domain Feature Extraction 25 2				
LIST OF TABLES VI				
LIST OF FIGURES				
LIST OF APPENDICES XiI		-	·-	
LIST OF ABBREVIATIONS				
CHAPTER 1 1. INTRODUCTION 1 1.1.1 Project Background 1 1.2 Problem statement 8 1.3 Research Objectives 9 1.4 Scope of Research 9 1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1 Electromyography Measurement 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 15 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3.1 Time Domain Feature Extraction 22 2.3.2 Frequency Domain Feature Extraction 25 2.3.3 Time-Frequency Domain Feature Extraction 28 2.3.3.1 Short-time Fourier Transform 28 2.3.3.2 Wavelet Transform 31 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittation Application on Biceps Brachii Musele 43 2.6 Summary 44 <td></td> <td></td> <td></td> <td></td>				
CHAPTER 1 1. INTRODUCTION 1 1.1. Project Background 1 1.2. Problem statement 8 1.3. Research Objectives 9 1.4. Scope of Research 9 1.5. Contribution of Research 10 1.6. Thesis Organization 10 2. LITERATURE REVIEW 12 2.1. Electromyography Measurement 12 2.1.1. Invasive Electromyography Technique 12 2.1.2. Non-Invasive Electromyography Technique 15 2.1.3. Advantages and Disadvantages of the Electromyography Measurement 17 2.2. Sources of Noise in Electromyography Signal 19 2.3. EMG Feature Extraction 21 2.3. EMG Feature Extraction 22 2.3. 2 Frequency Domain Feature Extraction 22 2.3. 3. Time-Frequency Domain Feature Extraction 28 2.3. 2. Wavelet Transform 28 2.3. 3. Wavelet Transform 31 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 3. METHODOLOGY 48 3.1 Experimental Design				
1. INTRODUCTION 1 1.1 Project Background 1 1.2 Problem statement 8 1.3 Research Objectives 9 1.4 Scope of Research 10 1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1 Electromyography Measurement 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 15 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3.1 Time Domain Feature Extraction 22 2.3.2 Frequency Domain Feature Extraction 25 2.3.3 Time-Frequency Domain Feature Extraction 25 2.3.3.1 Short-time Fourier Transform 29 2.3.3.2 Wavelet Transform 31 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 2.6 Summary 44 3. METHODOLOGY 48 3.1 Experimental Design	LIS	ST OF	PUBLICATIONS	xvii
1.1 Project Background 1 1.2 Problem statement 8 1.3 Research Objectives 9 1.4 Scope of Research 9 1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1 Electromyography Measurement 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 15 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3 EMG Feature Extraction 22 2.3.1 Time Domain Feature Extraction 25 2.3.2 Frequency Domain Feature Extraction 28 2.3.3.1 Short-time Fourier Transform 29 2.3.3.2 Wavelet Transform 31 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 <t< td=""><td>CH</td><td>IAPTI</td><td>$\mathbf{E}\mathbf{R}$</td><td>1</td></t<>	CH	IAPTI	$\mathbf{E}\mathbf{R}$	1
1.2 Problem statement 8 1.3 Research Objectives 9 1.4 Scope of Research 9 1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1 Electromyography Measurement 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 15 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3.1 Time Domain Feature Extraction 22 2.3.2 Frequency Domain Feature Extraction 25 2.3.3 Time-Frequency Domain Feature Extraction 28 2.3.3.1 Short-time Fourier Transform 29 2.3.3.2 Wavelet Transform 37 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 2.6 Summary 44 </td <td>1.</td> <td>INT</td> <td>RODUCTION</td> <td></td>	1.	INT	RODUCTION	
1.3 Research Objectives 9 1.4 Scope of Research 9 1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1 Electromyography Measurement 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 15 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3.1 Time Domain Feature Extraction 22 2.3.2 Frequency Domain Feature Extraction 25 2.3.3 Time-Frequency Domain Feature Extraction 28 2.3.3.1 Short-time Fourier Transform 29 2.3.3.2 Wavelet Transform 31 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 2.6 Summary 44 3.1 Experimental D			, e	1
1.4 Scope of Research 9 1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1 Electromyography Measurement 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 15 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3 1 Time Domain Feature Extraction 22 2.3.1 Time Domain Feature Extraction 25 2.3.2 Frequency Domain Feature Extraction 28 2.3.1 Short-time Fourier Transform 28 2.3.2 Wavelet Transform 31 2.3.3.2 Wavelet Packet Transform 37 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 2.6 Summary 44 3.1 Exp				
1.5 Contribution of Research 10 1.6 Thesis Organization 10 2. LITERATURE REVIEW 12 2.1 Electromyography Measurement 12 2.1.1 Invasive Electromyography Technique 12 2.1.2 Non-Invasive Electromyography Technique 15 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3 1 Time Domain Feature Extraction 22 2.3.1 Time Domain Feature Extraction 25 2.3.2 Frequency Domain Feature Extraction 28 2.3.3.1 Short-time Fourier Transform 29 2.3.3.2 Wavelet Transform 37 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 2.6 Summary 48 3.1 Experimental Design 49			· · · · · · · · · · · · · · · · · · ·	
1.6 Thesis Organization 2. LITERATURE REVIEW 2.1 Electromyography Measurement 2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 17 2.2 Sources of Noise in Electromyography Signal 2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3 Wavelet Transform 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.1 EMG Rehabilittaion Application on Biceps Brachii Muscle 3. METHODOLOGY 3.1 Experimental Design			±	
2.1 Electromyography Measurement 2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2 Sources of Noise in Electromyography Signal 2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.1 2.3.3.3 Wavelet Packet Transform 3.2 EMG Pattern Classification 3.3 Methodology 3.4 Experimental Design 3.5 Methodology 3.6 Experimental Design 4.7 Experimental Design				
2.1 Electromyography Measurement 2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2 Sources of Noise in Electromyography Signal 2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.1 2.3.3.3 Wavelet Packet Transform 3.2 EMG Pattern Classification 3.3 Methodology 3.4 Experimental Design 3.5 Methodology 3.6 Experimental Design 4.7 Experimental Design	2	LITI	FRATURE REVIEW	12
2.1.1 Invasive Electromyography Technique 2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2 Sources of Noise in Electromyography Signal 2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3 Wavelet Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.4 EMG Pattern Classification 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 2.6 Summary 3. METHODOLOGY 3.1 Experimental Design	4.			
2.1.2 Non-Invasive Electromyography Technique 2.1.3 Advantages and Disadvantages of the Electromyography Measurement 2.2 Sources of Noise in Electromyography Signal 2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.1 EMG Pattern Classification 3.2 EMG Rehabilitation Application on Biceps Brachii Muscle 3. METHODOLOGY 3.1 Experimental Design 48				
Measurement 17 2.2 Sources of Noise in Electromyography Signal 19 2.3 EMG Feature Extraction 21 2.3.1 Time Domain Feature Extraction 22 2.3.2 Frequency Domain Feature Extraction 25 2.3.3 Time-Frequency Domain Feature Extraction 28 2.3.3.1 Short-time Fourier Transform 29 2.3.3.2 Wavelet Transform 31 2.3.3.3 Wavelet Packet Transform 37 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 43 2.6 Summary 44 3. METHODOLOGY 48 3.1 Experimental Design 49			, , , , , , , , , , , , , , , , , , , 	15
2.2 Sources of Noise in Electromyography Signal 2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.1 EMG Pattern Classification 3.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 3.6 Summary 48 3. METHODOLOGY 3.1 Experimental Design			2.1.3 Advantages and Disadvantages of the Electromyography	
2.3 EMG Feature Extraction 2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.4 EMG Pattern Classification 3.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 3.6 Summary 3. METHODOLOGY 3.1 Experimental Design 48				
2.3.1 Time Domain Feature Extraction 2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.4 EMG Pattern Classification 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 2.6 Summary 3. METHODOLOGY 3.1 Experimental Design 48			, , , , ,	
2.3.2 Frequency Domain Feature Extraction 2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 2.4 EMG Pattern Classification 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 2.6 Summary 3. METHODOLOGY 3.1 Experimental Design 48		2.3		
2.3.3 Time-Frequency Domain Feature Extraction 2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 3.4 EMG Pattern Classification 3.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 3.6 Summary 3. METHODOLOGY 3.1 Experimental Design 48				
2.3.3.1 Short-time Fourier Transform 2.3.3.2 Wavelet Transform 3.3.3.3 Wavelet Packet Transform 2.4 EMG Pattern Classification 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 2.6 Summary 3. METHODOLOGY 3.1 Experimental Design 48			1 2	
2.3.3.2 Wavelet Transform 2.3.3.3 Wavelet Packet Transform 37 2.4 EMG Pattern Classification 39 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 2.6 Summary 3. METHODOLOGY 3.1 Experimental Design 48				
2.3.3.3 Wavelet Packet Transform 2.4 EMG Pattern Classification 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 2.6 Summary 37 48 3.1 Experimental Design				
2.4 EMG Pattern Classification 2.5 EMG Rehabilittaion Application on Biceps Brachii Muscle 2.6 Summary 39 43 43 44 3. METHODOLOGY 3.1 Experimental Design				
2.6 Summary 44 3. METHODOLOGY 48 3.1 Experimental Design 49		2.4		
3. METHODOLOGY 3.1 Experimental Design 49		2.5	EMG Rehabilittaion Application on Biceps Brachii Muscle	43
3.1 Experimental Design 49		2.6	Summary	44
1 6	3.			
3.3 Subjects and EMG Recording Procedure 51			<u> </u>	
3.4 EMG Data Collection 55			Subjects and EMG Recording Procedure	51 55

	3.5	Feature 1	Extraction		56
		3.5.1	Wavelet-I	Denoised Signal	56
			3.5.1.1	Mother Wavelet Optimal Selection	61
			3.5.1.2	Decomposition Levels	63
			3.5.1.3	Threshold Selection Rules	63
			3.5.1.4	Threshold Functions	64
			3.5.1.5	Thresholding Rescaling Methods	64
			3.5.1.6	Evaluation	65
		3.5.2	Extract Fe	eature Vector	65
			3.5.2.1	Root Mean Square Feature	67
			3.5.2.2	Mean Absolute Value Feature	67
			3.5.2.3	Autoregressive coefficient feature	67
	3.6	Linear V	ector Quant	ization	70
	3.7	Summar	У		72
4.	RES	ULT AND	DISCUSS!	ION	73
	4.1	Wavelet	-Denoising S	Signal Analysis	73
		4.1.1	Mother W	avelet Analysis	74
		4.1.2	Decompos	sition Levels Analysis	79
		4.1.3	Threshold	Rules Analysis and Threshold Function	81
		4.1.4	Threshold	Rescaling Analysis	87
	4.2	Extract 1	Feature Vect	or Analysis	88
		4.2.1	RMS Clas	ssification Accuracy	89
		4.2.2	MAV Cla	ssification Accuracy	91
		4.2.3	AR Covar	riance Classification Accuracy	94
	4.3	Compari	ison Between	n Three Techniques of Feature Extraction	96
	4.4	Biceps E	Brachii Reha	bilitation Application in Real Time Recognition	98
	4.5	Summar	У		101
5.	CONCLUSION			102	
	5.1	Conclus	ion		102
	5.2	Recomm	nendations		103
DE	FFDE	NCES			105
	REFERENCES APPENDICES			103	
		_ ~ ~~			

LIST OF TABLES

TABLE	TITLE	PAGE
2.1	Advantages and disadvantages of the electromyography	17
	measurement	
2.2	Summary of the previous research works on time domain features	23
2.3	Summary of the previous research works on frequency domain	25
	features	
2.4	Comparison of supervised learning algorithm applied WT for	42
	characterization of EMG signals	
2.5	Summary for three types of features extraction in the classification	45
	system	
3.1	Physical characteristic of the subjects	51
3.2	Levels of the arm angle positions	53
3.3	Type of resistance band loads	54
3.4	List of the mother wavelet families	62
3.5	Thresholding rules	64
4.1	Mean square error performance for 21 mother wavelets function	76
4.2	Signal to noise ratio performance for 21 mother wavelets function	78
4.3	Mean square error performance of four threshold rules in	82
	Daubechies family	
4.4	Signal to noise ratio performance of four threshold rules in	83
	Daubechies family	

4.5	Mean square error performance of four threshold rules in Symlets	84
	family	
4.6	Signal to noise ratio performance of four threshold rules in	85
	Symlets family	
4.7	Mean square error performance of four threshold rules in Coiflet	86
	family	
4.8	Signal to noise ratio performance of four threshold rules in Coiflet	87
	family	
4.9	Training data sets performance for female subjects using RMS	89
	feature	
4.10	Training data sets performance for male subjects using RMS	89
	feature	
4.11	Classification accuracy performance of the RMS test data	90
4.12	Training data sets performance for female subjects using MAV	92
	feature	
4.13	Training data sets performance for male subjects using MAV	92
	feature	
4.14	Classification accuracy performance of the MAV testing results	93
4.15	Training data sets performance for female subjects using AR	94
	covariance feature	
4.16	Training Data sets performance for male subjects using AR	94
	covariance feature	
4.17	Classification accuracy performance of the AR covariance test	95
	data	

4.18	Performance of the classification for three different combination	97
	techniques	
4.19	Results of the train data in the real-time application system	99
4.20	Classification accuracy performance for real-time application	99
	system	

LIST OF FIGURES

FIGURE	TITLE	PAGE
1.1	Electroencephalography signal recording	2
1.2	Electrocardiography signal of heartbeats	4
1.3	Measuring electromyography signal	5
1.4	The technique of measuring	6
2.1	Concentric needle electrode	13
2.2	Monopolar needle electrode	14
2.3	Single fiber electrode	14
2.4	Schematic diagram of the fine wire	15
2.5	Gelled electromyography electrode	16
2.6	Dry electromyography electrodes	17
2.7	Input function of short-time Fourier Transform parameter	30
2.8	Process of discrete wavelet transform analysis	35
2.9	Process of wavelet packet transform	38
3.1	Process flow electromyography signal classification	48
3.2	Real time rehabilitation assessment system	48
3.3	Research flowchart for the first stage	50
3.4	Location of the electromyography electrodes	52
3.5	LabVIEW program to record the raw electromyography signal	55
3.6	LabVIEW program for denoising signal	56
3.7	Discrete wavelet transform decomposition steps	59
3.8	Inverse discrete wavelet transform reconstruction steps	60

3.9	Several mother wavelets function	62
3.10	Sliding window analysis	66
3.11	Linear vector quantization network architecture	70
4.1	Analysis of mean square error for 21 mother wavelets function	75
4.2	Analysis of signal to noise ratio for 21 mother wavelets function	77
4.3	Mean square error performance of Daubechies6 for 13	79
	decomposition levels	
4.4	Signal to noise ratio performance of Daubechies6 for 13	80
	decomposition levels	
4.5	Analysis mean square error of four threshold rules in Daubechies	81
	family	
4.6	Analysis signal to noise ratio four threshold rules in Daubechies	82
	family	
4.7	Analysis mean square error of four threshold rules in Symlets	83
	family	
4.8	Analysis signal to noise ratio of four threshold rules in Symlets	84
	family	
4.9	Analysis mean square error of four threshold rules in Coiflet	85
	family	
4.10	Analysis signal to noise ratio of four threshold rules in Coiflet	86
	family	
4.11	Threshold rescaling performance	88
4.12	Classification accuracy for three different combination techniques	96

4.13	Graphical user interface for biceps brachii muscle rehabilitation	98
	application system	
4.14	Real-time recognition system	100

LIST OF APPENDICES

APPENDIX	TITLE	PAGE
A	Real-time rehabilitation application system for biceps brachii	122
	muscle at 30°	
В	Real-time rehabilitation application system for biceps brachii	123
	muscle at 90°	
C	Real-time rehabilitation application system for biceps brachii	124
	muscle at 150°	

LIST OF ABBREVIATIONS

EEG - Electroencephalography

ECG - Electrocardiography

ENG - Electronystagmography

EMG - Electromyography

CNS - Central Nervous System

MUAP - Motor Unit Action Potential

MUAPTs - Motor Unit Action Potential Trains

kNN - k-Nearest Neighbors

HMM - Hidden Markov Model

ANN - Artificial Neural Network

LVQ - Linear Vector Quantization

CNN - Convolutional Neural Network

SVM - Support Vector Machine

LDA - Linear Discriminant Analysis

SENIAM - Surface Electromyography for non-invasive Assessment of Muscles

Ag-AgCI - silver-silver chloride

TD - Time Domain

FD - Frequency Domain

TFD - Time-Frequency Domain

MAV - Mean Absolute Value

MAVS - Mean Absolute Value Slope

ZC - Zero Crossings

SSC - Slope Sign Changes

SSI - Simple Square Integral

VAR - Variance of EMG

RMS - Root Mean Square

WAMP - William Amplitude

IAV - Integrated Absolute Value

MYOP - Myopulse percentage rate

AR - Autoregressive

TM - Temporal Moment

WL - Waveform Length

PSD - Power Spectral Density

MNF - Mean Frequency

MDF - Median Frequency

PKF - Peak Frequency

MNP - Mean Power

TTP - Total Power

SM - Spectral Moment

FR - Frequency Ratio

PSR - Power Spectrum Ratio

VCF - Variance of Central Frequency

STFT - short-time Fourier Transform

WT - Wavelet Transform

WPT - Wavelet Packet Transform

CWT - Continuous Wavelet Transform

DWT - Discrete Wavelet Transform

LIST OF SYMBOLS

W_n	-	Window	function
'' n			

 S_n - Time-shift

τ - Modulation

t - Translation parameters

 $\psi(t)$ - Mother wavelet function

 $\phi(t)$ - Scaling function

h(n) - Low-pass filter

g(n) - High-pass filter

x(n) - Noise EMG signal

 cA_n - Approximation coefficient

 cD_n - Detail Coefficient

 σ^2 - Variance

LIST OF PUBLICATIONS

Journals

- Burhan, N., Kasno, M.A., Ghazali, R., Jali, M.H., Said, M.R., 2017. Discrete
 Wavelet Transform Approach on the Electromyography Signal in Rehabilitation
 Exercise. *International Journals of Basic & Applied Sciences IJBAS IJENS*, 17(3),
 pp. 1-6.
- 2. **Burhan, N.,** Kasno, M.A., Ghazali, R., Jali, M.H., Said, M.R., 2017. Analysis of the Biceps Brachii Muscle Activity by Varying the Arm Movement Level and Load Resistance Band. *Journal of Health Engineering*, 2017, pp. 1-8.

Conferences

- Burhan, N., Kasno, M.A., Ghazali, R., 2016. Feature Extraction of Surface Electromyography (sEMG) and Signal Processing Technique in Wavelet Transform: A Review, *IEEE International Conference on Automatic Control and Intelligent* Systems, pp. 141-146.
- Burhan, N., Kasno, M.A., Ghazali, R., Jali, M.H., Said, M.R., 2017.
 Electromyography Signal Analysis using Wavelet Transform Approach for Resistance Band Rehabilitation. *Proceeding Mechanical Engineering Research Day* 2017, pp. 99-100.

CHAPTER 1

INTRODUCTION

The present chapter discusses the concept of biomedical signals, with emphasis on electromyography as a diagnosis process of the human muscle health and the problems occurred during electromyography signal processing and its rehabilitation applications. The chapter also covers the objectives of the study, its scopes and contribution of the research on spectral estimation and supervised classification technique for real time surface electromyography pattern recognition.

1.1 Project Background

With the advance of science and technology, there has been a quantum leap in the development of automated and semi-automated systems supporting physiotherapy and rehabilitation. The purpose of these system development is to assist patients' recovery from health issues and to return to their previous state of health. Rehabilitation treatments are usually used by patients after a major operation, chronic pain, stroke, or severe accident that caused injury to any body part. The human body consists of many component systems involving biomedical signals such as the nervous system, cardiovascular system, and musculoskeletal system.

The rehabilitation system for biomedical signal-based device generally contains a biomedical signal sensor to detect the different types of biomedical signals. Biomedical signal is an observation of physiological activities and is crucial as a collective electrical signal of the human organ part. Basically, the biomedical signals can be classified into four types: electroencephalography (EEG), electrocardiography (ECG), electronystagmography (ENG), and electromyography (EMG). Each of these biomedical signals has their own specifications that are used to measure the electrical signals for different types of organ parts.

The oldest technique in biomedical signal that had been practiced in clinical situation is the EEG as shown in Figure 1.1. This is a method for recording the electrical activity of brain either in healthy or diseased conditions using small, flat metal discs or electrodes attached to the scalp (Millett et al., 2015). This method represents the graphics of the electrical potential generated by the cerebrum. Essentially, the brain is the major part which controls and coordinates the entire parts of the human body such as muscles and nerves. It is necessary to identify the function and cognitive behavior of the human brain in order to find out the good solution related to brain issues.

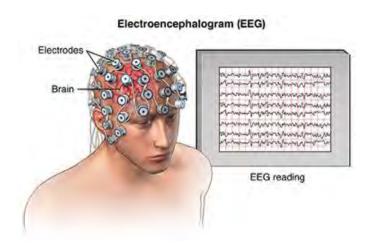


Figure 1.1 Electroencephalography signal recording (Millett et al., 2015)

Basically, the brain is divided into two parts which are right part and left the part.

The two parts mutually control each other, where the left part of the brain is liable for